

US-PAT-NO: 5824040

DOCUMENT-IDENTIFIER: US 5824040 A

TITLE: Endoluminal prostheses and therapies  
for highly variable  
body lumens

----- KWIC -----

Detailed Description Text - DETX (22):

A method of fabricating a helical stent-graft 71 will be described with reference to FIG. 5E. A series of linked diamond-shaped elements 73 are first attached to a strip of liner material 75, typically being stitched with a sewing machine. The ribbon is then wound over a mandrel 77 of the desired size, and adjacent edges of the ribbon are sewn to each other (or otherwise permanently joined). Such a method may be substantially automated and continuous, and is thus particularly beneficial for producing a large number of prostheses. The helical stent-graft may optionally be cut to length, but will preferably include a crown stitched stent-ring 79 for sealing and ends against a surrounding lumen when deployed therein.

L Number	Hits	Search Text	DB	Time stamp
1	0	(measure or measuring) with aneurysm and stent and restrict\$3 near3 (dilation or expansion or expand)	USPAT; US-PGPUB; EPO; JPO; DERWENT	2003/09/05 14:46
2	43	(measure or measuring) with aneurysm and stent	USPAT; US-PGPUB; EPO; JPO; DERWENT	2003/09/05 14:57
3	74	(623/903).CCLS.	USPAT; US-PGPUB; EPO; JPO; DERWENT	2003/09/05 15:26
4	385	(623/1.13).CCLS.	USPAT; US-PGPUB; EPO; JPO; DERWENT	2003/09/05 15:46
5	118	(623/1.23).CCLS.	USPAT; US-PGPUB; EPO; JPO; DERWENT	2003/09/05 15:58
6	38	((measure or measuring) with aneurysm and stent) or ((623/903).CCLS.) or ((623/1.13).CCLS.) or ((623/1.23).CCLS.))	USPAT; US-PGPUB; EPO; JPO; DERWENT	2003/09/05 16:13
7	992	and (limit or limited) near3 expansion 623/1.15	USPAT; US-PGPUB; EPO; JPO; DERWENT	2003/09/05 16:14
8	47	("3304557"   "3316557"   "3945052"   "4299015"   "4652263"   "4670286"   "4731073"   "4834755"   "4922905"   "5037377"   "5064435"   "5084065"   "5123917"   "5133742"   "5163952"   "5258042"   "5282847"   "5330500"   "5387621"   "5413598"   "5443499"   "5443500"   "5456713"   "5470313"   "5476507"   "5496364"   "5507770"   "5527353"   "5545209"   "5545210"   "5556413"   "5556426"   "5562725"   "5562727"   "5591195"   "5591199"   "5609605"   "5617878"   "5683451"   "5769882"   "5824037"   "5843158"   "6019786"   "6123722"   "6176875"   "6283991"   "6361557").PN.	USPAT	2003/09/05 16:38

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# United States Patent (19)

(11) Patent Number: 5,556,413  
(43) Date of Patent: Sep. 17, 1996

## [54] COILED STENT WITH LOCKING ENDS

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[75] Inventor: Sharon Lam, San Jose, Calif.  
[73] Assignee: Advanced Cardiovascular Systems, Inc., Santa Clara, Calif.

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[21] Appl. No.: 209,827

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[22] Filed: Mar. 11, 1994  
[51] Int. Cl. A61M 28/00  
[52] U.S. Cl. 606/198; 623/1; 623/12  
[58] Field of Search: 606/198, 108, 104, 105; 623/1, 12; 128/856

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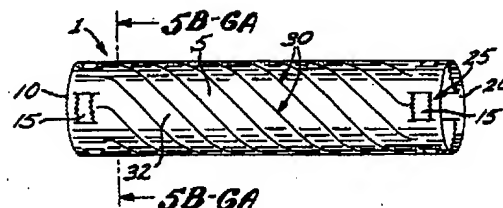
Primary Examiner—Gary Jackson  
Assistant Examiner—William W. Lewis  
Attorney, Agent, or Firm—Fulwider Patton Lee & Utecht

## [57] ABSTRACT

An intravascular stent comprising a cylindrical body capable of expansion having end assemblies capable of locking in an expanded state. The end assemblies may have a series of tabs and apertures that interlock and rotate as the stent ends expand to an open position to support a section of vasculature or other body lumen. The stent is bio-compatible, may be bio-erodible, and capable of localized drug delivery.

(List continued on next page.)

27 Claims, 9 Drawing Sheets



File Edit View Tools Window Help

	Document ID	Class	Issue Date	Page	Title
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48	US 6190397 B1	U	20010220	55	Means an
49	US 6206912 B1	U	20010327	39	Medical
50	US 20010011189	U	20010802	57	In situ
51	US 20010025195	U	20010927	44	Flexible

## United States Patent [19]

Lazarus

 Patent Number: 5,397,345  
 Date of Patent: Mar. 14, 1995

## [54] ARTIFICIAL GRAFT AND IMPLANTATION METHOD

[75] Inventor: Harrison M. Lazarus, Salt Lake City, Utah

[73] Assignee: EndoVascular Technologies, Inc., Menlo Park, Calif.

[21] Appl. No.: 175,491

[22] Filed: Dec. 29, 1993

## Related U.S. Application Data

[60] Continuation of Ser. No. 34,587, Mar. 22, 1993, abandoned, which is a continuation of Ser. No. 732,058, Aug. 29, 1991, abandoned, which is a division of Ser. No. 166,059, Mar. 9, 1988, Pat. No. 5,104,399, which is a continuation-in-part of Ser. No. 946,507, Dec. 10, 1986, Pat. No. 4,787,899, which is a continuation of Ser. No. 339,933, Dec. 9, 1983, abandoned.

[51] Int. Cl.<sup>6</sup> ..... A61F 2/06; A61F 2/54; A61B 17/00; A61B 29/00  
 [52] U.S. Cl. .... 623/1; 606/153; 606/194; 604/95; 623/66  
 [58] Field of Search ..... 604/96, 104; 606/153, 606/158, 191, 192, 194, 195; 623/1, 2, 11, 66

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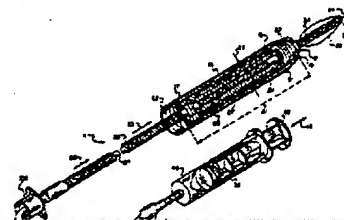
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Primary Examiner—Randall L. Green  
 Assistant Examiner—Elizabeth M. Burke  
 Attorney Agent or Firm—Folwider, Patton, Lee & Utech

## [57] ABSTRACT

An intraluminal grafting system includes a hollow graft which has a proximal staple positioned proximate its proximal end and a distal staple adapted proximate its distal end. The system includes a capsule for transporting the graft through the lumen and for positioning the proximal end of the graft upstream in a lumen which may be a blood vessel or artery. A tube is connected to the capsule and extends to exterior the vessel for manipulation by the user. A catheter is positioned within the tube to extend from the cavity and through the graft to exterior the body. The catheter has an inflatable membrane or balloon proximate the distal end thereof which is in communication via a channel with inflation and deflation means located exterior the vessel. With the inflatable membrane deflated, the capsule is positioned in the lumen and manipulated to a desired location. The inflatable membrane is manipulated by the rod away from the graft. The force exerted by the inflatable membrane and the structure of the staples urges the staples in the vessel wall, retaining the graft in position. The remainder of the intraluminal grafting system is then removed from the corporeal vessel.

10 Claims, 3 Drawing Sheets



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49	US 6206912 B1	U	20010327	39	Medical
50	US 20010011189	U	20010802	57	In situ
51	US 20010025195	U	20010927	44	Flexibly



US 5925076A

## United States Patent [19]

Inoue

[11] Patent Number: 5,925,076

[45] Date of Patent: \*Jul. 20, 1999

[54] APPLIANCE TO BE IMPLANTED, METHOD OF COLLAPSING THE APPLIANCE TO BE IMPLANTED AND METHOD OF USING THE APPLIANCE TO BE IMPLANTED

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[76] Inventor: Kanji Inoue, 98-13, Miyazaki-cho  
Shimogamo, Kyoto, Japan

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[\*] Notice: This patent is subject to a terminal disclaimer.

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[21] Appl. No.: 08/898,427

[22] Filed: Jul. 22, 1997

## Related U.S. Application Data

[62] Division of application No. 08/765,215, Jan. 3, 1997, Pat. No. 5,843,162

Primary Examiner—Paul B. Prebille  
Assistant Examiner—Tam A. Nguyen  
Attorney, Agent, or Firm—Barnes & Wozniak, Ltd.

## [57] ABSTRACT

[30] Foreign Application Priority Data

May 19, 1995 [JP] Japan PC1995-00972

[51] Int. Cl. A61F 2/36

[52] U.S. Cl. 623/1; 623/12; 606/105; 606/138

[58] Field of Search 623/1, 11, 12; 606/198, 195, 196, 191, 108

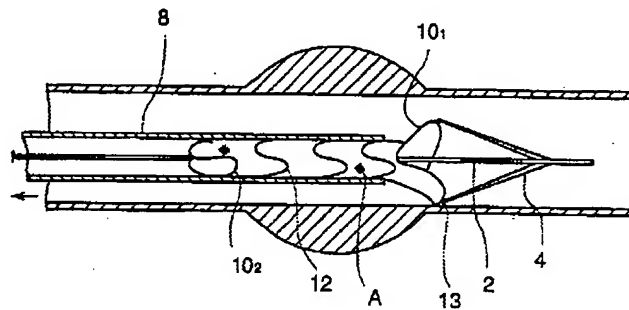
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A collapsible artificial blood vessel A comprises a flexible front end wire ring 10<sub>1</sub>, a flexible rear end wire ring 10<sub>2</sub> arranged facing to the front end wire ring, a tubular cover 7 which connects the end wire rings, and a plurality of intermediate wire rings 12 arranged spaced apart from each other between the front end wire ring and the rear end wire ring. The circumference of the front end wire ring is equally divided into four segments by dividing points 411, 421, 431, 441. Hooks 13 are formed for a front pull string to be passed through at the dividing points 411, 431. The circumference of the intermediate wire rings are fixed to the tubular cover 7 by suturing or with adhesive at the positions 512, 522, 532 and 542. The device is collapsed for use by folding the wire rings and insertion of the device into a funnel tube.

6 Claims, 49 Drawing Sheets



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82	US 20030023299	U	20030130	16	Reposition	
83	US 6511505 B2	U	20030128	16	Variable st	
84	US 20030018378	U	20030123	16	Endovascu	
85	US 6508835 B1	U	20030121	37	Endolumina	
86	US 20030009213	U	20030109	12	Stent havi	
87	US 20030009212	U	20030109	20	Axially-co	
88	US 20030009211	U	20030109	17	Implant ha	
89	US 20030009210	U	20030109	11	ePTFE graf	
90	US 20030006528	U	20030109	16	Methods fo	
91	US 20030004562	U	20030102	13	Endolumina	
92	US 6500203 B1	U	20021231	25	Process fo	
93	US 20020198588	U	20021226	28	Covered end	
94	US 20020198587	U	20021226	19	Modular st	
95	US 20020198586	U	20021226	47	APPLIANCE	
96	US 6497722 B1	U	20021224	10	Methods and	
97	US 20020193864	U	20021219	18	Coiled shee	
98	US 6494909 B2	U	20021217	14	Endovascu	
99	US 6488701 B1	U	20021203	16	Stent-graf	
100	US 6485513 B1	U	20021126	10	Percutaneo	
101	US 20020173836	U	20021121	12	Method of	
102	US 6482227 B1	U	20021119	27	Stent graf	
103	US 20020169497	U	20021114	36	Endovascu	
104	US 20020169496	U	20021114	19	Methods for	
105	US 6478813 B1	U	20021112	37	Method for	
106	US 20020165603	U	20021107	43	Kink-resis	
107	US 20020165602	U	20021107	23	Self expand	



US 20020165603A1

(19) United States

(12) Patent Application Publication  
Thornton et al.

(10) Pub. No.: US 2002/0165603 A1  
(43) Pub. Date: Nov. 7, 2002

(54) KINK-RESISTANT BIFURCATED  
PROSTHESIS

Publication Classification

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(51) Int. Cl.<sup>7</sup> A61F 2/06  
(52) U.S. Cl. 623/1.13; 623/1.22; 623/1.35;  
623/1.36

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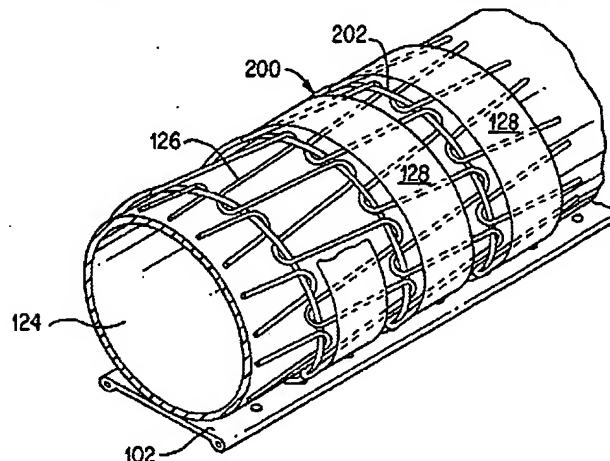
(57) ABSTRACT

(21) Appl. No.: 10/184,989  
(22) Filed: Jul. 1, 2002

Related U.S. Application Data

(63) Continuation of application No. 08/772,372, filed on  
Dec. 23, 1996.

The invention consists of an endoluminal prosthesis adapted for placement at a bifurcation site within the body. The stent or stent-graft may be constructed to have segments of differing structural properties. A section of the stent-graft may be constructed to have a single-lumen tubular stent member covering a multi-lumen graft member. The stent-graft may comprise at least two modular components adapted for in situ assembly. An extended cylindrical interference fit may be used to seal the modular components.



	Document ID	KS	Issue	Da	Page	Title
64	US 20030055484	U	20030320	20		Exterior st
65	US 6530950 B1	U	20030311	14		Intralumin
66	US 20030045926	U	20030306	10		Self artic
67	US 6524337 B1	U	20030225	6		Intralumin
68	US 6524335 B1	U	20030225	14		Endolumina
69	US 6524334 B1	U	20030225	12		Expandable
70	US 6520986 B2	U	20030218	34		Kink resist
71	US 20030033002	U	20030213	14		Aorto uni-
72	US 6517573 B1	U	20030211	10		Hook for a
73	US 6517572 B2	U	20030211	39		Endovascu
74	US 6517571 B1	U	20030211	25		Vascular g
75	US 6517570 B1	U	20030211	22		Exterior st
76	US 20030028246	U	20030206	15		Compliant
77	US 20030028240	U	20030206	16		Stent-graft
78	US 20030028239	U	20030206	22		LOW PROFILE
79	US 6514283 B2	U	20030204	10		Intralumin
80	US 6514282 B1	U	20030204	35		Method of
81	US 20030023300	U	20030130	16		Endolumina
82	US 20030023299	U	20030130	16		Reposition
83	US 6511505 B2	U	20030128	16		Variable st
84	US 20030018378	U	20030123	16		Endovascu
85	US 6508835 B1	U	20030121	37		Endolumina
86	US 20030009213	U	20030109	12		Stent havin
87	US 20030009212	U	20030109	20		Axially-co
88	US 20030009211	U	20030109	17		Implant hav
89	US 20030009210	U	20030109	11		ePTFE graft
90	US 20030006528	U	20030109	16		Methods for
91	US 20030004562	U	20030102	13		Endolumina
92	US 6500203 B1	U	20021231	25		Process for
93	US 20020198588	U	20021226	28		Covered end
94	US 20020198587	U	20021226	19		Modular st
95	US 20020198586	U	20021226	47		APPLIANCE
96	US 6497722 B1	U	20021224	10		Methods and
97	US 20020193864	U	20021219	18		Coiled shee
98	US 6494909 B2	U	20021217	14		Endovascu
99	US 6488701 B1	U	20021203	16		Stent-graft
100	US 6485513 B1	U	20021126	10		Percutaneou
101	US 20020173836	U	20021121	12		Method of
102	US 6482227 B1	U	20021119	27		Stent graft
103	US 20020169497	U	20021114	36		Endovascu
104	US 20020169496	U	20021114	19		Methods for
105	US 6478813 B1	U	20021112	37		Method for
106	US 20020165603	U	20021107	42		Kink-resist
107	US 20020165602	U	20021107	23		Self expand
108	US 20020165601	U	20021107	11		Bioabsorba
109	US 6475232 B1	U	20021105	12		Stent with
110	US 20020156523	U	20021024	22		Exterior st
111	US 20020156522	U	20021024	10		Aortic gra
112	US 20020156521	U	20021024	25		Bifurcated
113	US 20020156518	U	20021024	15		Branched a
114	US 6468301 B1	U	20021022	15		Reposition
115	US 6468300 B1	U	20021022	5		Stent cover
116	US 20020151958	U	20021017	14		Large vesse
117	US 20020151957	U	20021017	20		Axially-co
118	US 6464719 B2	U	20021015	6		Low profile
119	US 20020147492	U	20021010	22		Endolumina
120	US 6461320 B1	U	20021008	34		Method and



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(19) United States

(12) Patent Application Publication  
Shokooht et al.

(10) Pub. No.: US 2002/0147492 A1  
(43) Pub. Date: Oct. 10, 2002

(54) ENDOLUMINAL VASCULAR PROSTHESIS

Related U.S. Application Data

(76) Inventors: Mehrdad M. Shokooht, Rancho Palos Verdes, CA (US); Michael R. Henson, Trabuco Canyon, CA (US); Gerard von Hoffmann, Trabuco Canyon, CA (US)

(53) Continuation of application No. 09/483,411, filed on Jan. 14, 2000, now Pat. No. 6,331,190, which is a continuation of application No. 09/034,689, filed on Mar. 4, 1998, now Pat. No. 6,077,296.

Publication Classification

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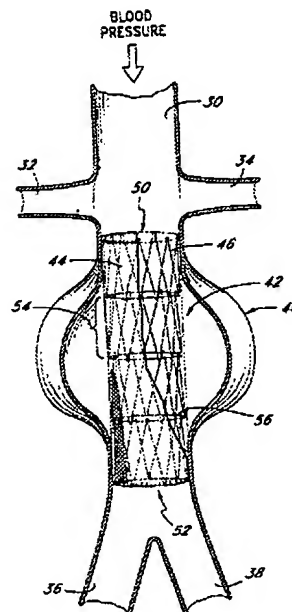
(51) Int. Cl.<sup>7</sup> A61F 2/06  
(52) U.S. Cl. 623/1.13; 623/1.16

(57) ABSTRACT

Disclosed is a tubular endoluminal vascular prosthesis, useful in treating, for example, an abdominal aortic aneurysm. The prosthesis comprises a self expandable wire support structure surrounded by a flexible tubular membrane. A delivery catheter and methods are also disclosed.

(21) Appl. No.: 10/032,230

(22) Filed: Dec. 18, 2001





	Document ID	KS	Issue	Da	Page	Title
124	US 6451051 B2	U	20020917	100	Intravascu	
125	US 6451048 B1	U	20020917	25	Wire connec	
126	US 6451047 B2	U	20020917	16	Encapsulat	
127	US 20020128703	U	20020912	8	METHOD AND	
128	US 20020123789	U	20020905	10	Stent cover	
129	US 20020123788	U	20020905	10	Sheath for	
130	US 6443981 B1	U	20020903	12	Expandable	
131	US 20020116048	U	20020822	16	Endovascu	
132	US 6436132 B1	U	20020820	10	Composite	
133	US 20020111668	U	20020815	9	Seamless b	
134	US 20020111667	U	20020815	14	Non-expand	
135	US 6432131 B1	U	20020813	8	Method and	
136	US 20020107565	U	20020808	15	Endovascu	
137	US 6428550 B1	U	20020806	34	Sutureless	
138	US 20020103527	U	20020801	13	Stent with	
139	US 20020095205	U	20020718	7	Encapsulat	
140	US 20020095140	U	20020718	15	Reposition	
141	US 20020091437	U	20020711	12	Polymer co	
142	US 6416537 B1	U	20020709	7	Multi-stage	
143	US 20020082675	U	20020627	10	Intralumin	
144	US 20020082674	U	20020627	9	Surgical g	
145	US 20020077693	U	20020620	21	Covered, co	
146	US 20020068967	U	20020606	104	Intravascu	
147	US 6398803 B1	U	20020604	7	Partial enc	
148	US 6398802 B1	U	20020604	15	Low profile	
149	US 20020065546	U	20020530	14	Stent graft	
150	US 6395022 B1	U	20020528	13	Endovascu	
151	US 6395019 B2	U	20020528	20	Endovascu	
152	US 6395018 B1	U	20020528	21	Endovascu	
153	US 20020062147	U	20020523	17	Stent havin	
154	US 20020062146	U	20020523	38	Methods and	
155	US 6390098 B1	U	20020521	25	Percutaneo	
156	US 20020058993	U	20020516	37	Supra-rena	
157	US 20020058987	U	20020516	33	Bilateral	
158	US 20020058986	U	20020516	33	Stent graft	
159	US 20020058985	U	20020516	22	Thoracic a	
160	US 20020058984	U	20020516	28	Extension	
161	US 20020055769	U	20020509	13	Stent with	
162	US 20020055768	U	20020509	13	METHOD OF	
163	US 6383214 B1	U	20020507	15	Encapsulat	
164	US 6383171 B1	U	20020507	36	Methods and	
165	US 20020052645	U	20020502	18	Endovascu	
166	US 20020052644	U	20020502	46	Implantabl	
167	US 20020052643	U	20020502	22	Tapered enc	
168	US 6379382 B1	U	20020430	10	Stent havin	
169	US 20020049489	U	20020425	7	Prosthesis	
170	US 6375675 B2	U	20020423	48	Methods and	
171	US 20020045931	U	20020418	10	Support str	
172	US 6371982 B2	U	20020416	11	Graft struc	
173	US 6371981 B1	U	20020416	14	Vascular g	
174	US 20020042646	U	20020411	7	Stent devic	
175	US 20020042645	U	20020411	27	Drug eluti	
176	US 20020042644	U	20020411	11	Bifurcated	
177	US 6368345 B1	U	20020409	49	Methods and	
178	US 20020040237	U	20020404	9	ePTFE graf	
179	US 20020040236	U	20020404	27	PROCEDURES	
180	US 20020040235	U	20020404	11	Endovascu	



(19) United States

(12) Patent Application Publication  
LAU et al.

(10) Pub. No.: US 2002/0040236 A1  
(43) Pub. Date: Apr. 4, 2002

(54) PROCEDURES FOR INTRODUCING STENTS  
AND STENT-GRAFTS

(52) U.S. Cl. 623/1.12; 623/1.13; 623/1.17;  
623/1.2; 623/1.23

(75) Inventors: LILIP LAU, SUNNYVALE, CA (US);  
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(57) ABSTRACT

This invention is a medical device and a method of using it. The device is a foldable stent or stent-graft which may be percutaneously delivered with (or on) a catheter, typically an endovascular catheter, to a body cavity or lumen and then expanded. It may also be delivered or via surgical (or other) techniques. The expandable stent structure utilizes rotational members which distribute bending and folding loads in such a way that the stent is not plastically deformed. The stent's configuration allows it to be folded or otherwise compressed to a very small diameter prior to deployment without changing the length of the stent. The graft component cooperating with the stent is tubular and preferably is blood-compatible material which may, if desired, be reinforced with fibers. The stent is able to provide collapsible support for otherwise fragile graft material.

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(\*) Notice: This is a publication of a continued prosecution application (CPA) filed under 37 CFR 1.53(d).

(21) Appl. No.: 08/896,373

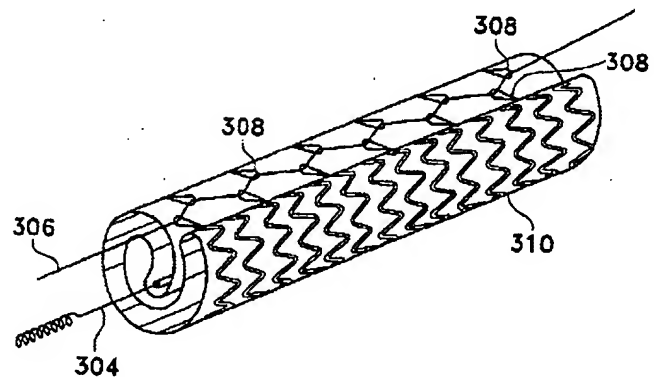
(22) Filed: Jul. 18, 1997

Related U.S. Application Data

(63) Continuation of application No. 08/754,398, filed on Nov. 20, 1996, now abandoned.

Publication Classification

(51) Int. Cl. A61F 2/06





	Document ID	KS	Issue	Pa	Title
186	US 6361557 B1	U	20020326	18	Staplebutt
187	US 20020035395	U	20020321	26	Implantabl
188	US 20020035394	U	20020321	23	Methods and
189	US 6357104 B1	U	20020319	9	Method of
190	US 20020032487	U	20020314	17	Prosthesis
191	US 6355056 B1	U	20020312	8	Implantabl
192	US 6355055 B1	U	20020312	8	Endovascu
193	US 20020026231	U	20020228	16	Radially ex
194	US 20020026230	U	20020228	27	Removable
195	US 20020026137	U	20020228	31	Method and
196	US 20020019665	U	20020214	48	Methods and
197	US 6346119 B1	U	20020212	8	Graft equi
198	US 20020016627	U	20020207	13	Tubular st
199	US 20020016626	U	20020207	10	Intralumin
200	US 20020016625	U	20020207	12	Drug/drug
201	US 6344054 B1	U	20020205	7	Endolumina
202	US 6340366 B1	U	20020122	15	Stent with
203	US 20020007208	U	20020117	11	Device with
204	US 20020004677	U	20020110	6	Low profil
205	US 6336937 B1	U	20020108	27	Multi-stage
206	US 6334869 B1	U	20020101	25	Endolumina
207	US 6334868 B1	U	20020101	6	Stent cover
208	US 6334867 B1	U	20020101	7	Surgical g
209	US 20010053930	U	20011220	41	Endovascu
210	US 6331527 B1	U	20011218	69	Promoter s
211	US 6331188 B1	U	20011218	22	Exterior s
212	US 20010049550	U	20011206	31	METHOD OF
213	US 6325820 B1	U	20011204	14	Coiled she
214	US 20010047198	U	20011129	104	Intravascu
215	US 20010044647	U	20011122	13	Modular enc
216	US 6319278 B1	U	20011120	9	Low profil
217	US 6319277 B1	U	20011120	10	Nested ste
218	US 20010041928	U	20011115	7	Endovascu
219	US 20010041927	U	20011115	7	By-pass ar
220	US 6315792 B1	U	20011113	34	Remotely r
221	US 6315791 B1	U	20011113	15	Self-expa
222	US 20010039446	U	20011108	20	ENCAPSULAT
223	US 6312458 B1	U	20011106	14	Tubular st
224	US 6312457 B1	U	20011106	10	Intralumin
225	US 6312456 B1	U	20011106	7	Biocompatil
226	US 20010037142	U	20011101	16	Endovascu
227	US 20010037139	U	20011101	31	Method and
228	US 6309413 B1	U	20011030	12	Expandable
229	US 6309343 B1	U	20011030	9	Method for
230	US 20010032009	U	20011018	7	Partial enc
231	US 20010027338	U	20011004	11	Endovascu
232	US 6296661 B1	U	20011002	21	Self-expa
233	US 20010025195	U	20010927	44	Flexible v
234	US 20010025131	U	20010927	13	Methods fo
235	US 6293965 B1	U	20010925	24	Tubular mec
236	US 20010023370	U	20010920	12	COMPOSITE
237	US 6290720 B1	U	20010918	13	Stretchabl
238	US 20010021870	U	20010913	13	Externally
239	US 6287330 B1	U	20010911	37	Aortoiliac
240	US 20010020182	U	20010906	26	Expandable
241	US 20010020181	U	20010906	7	PARTIAL EN
242	US 6292001 B1	U	20010904	34	Endolumina



US 20010020181A1

(19) United States

(12) Patent Application Publication (10) Pub. No.: US 2001/0020181 A1  
LAYNE (43) Pub. Date: Sep. 6, 2001

(54) PARTIAL ENCAPSULATION OF STENTS  
USING STRIPS AND BANDS

(52) U.S. Cl. 623/1.13; 623/1.16; 623/1.49

(76) Inventor: RICHARD LAYNE, PHOENIX, AZ  
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(57) ABSTRACT

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(\*) Notice: This is a publication of a continued prosecution application (CPA) filed under 37 CFR 1.53(d).

Partially encapsulated stents are made using strips and bands of covering material. In one embodiment, ringed stents are placed over an inner ePTFE tube (e.g., supported on a mandrel) and are covered by a series of longitudinal strips. A series of spaced apart ePTFE circumferential bands can then be placed over the top of the longitudinal strips and ringed stents; alternatively bands alone or strips alone may be employed. All of the components of the structure are then laminated to the inner ePTFE tube to capture the stent. By selecting the size and position of the ePTFE bands, it is possible to leave critical parts of the stent unencapsulated to facilitate flexibility and expansion. The longitudinal strips can be woven about the stent and later laminated into position to provide an anti-compression function as well as overall structural stability. Although a single stent can be used, these approaches lend themselves to use of a plurality of individual ring stents spaced apart along the inner ePTFE tube.

(21) Appl. No.: 09/408,890

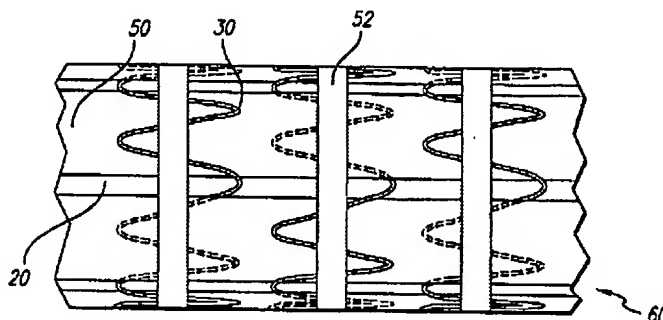
(22) Filed: Sep. 29, 1999

Related U.S. Application Data

(63) Non-provisional of provisional application No. 60/118,269, filed on Feb. 2, 1999.

Publication Classification

(51) Int. Cl.7 A61F 2/06



File Edit View Tools Window Help

	Document ID	Issue-Date	Page	Title
1	US 5123917 A	U 19920623	9	Expandab
2	US 5443499 A	U 19950822	11	Radially
3	US 5653746 A	U 19970805	11	Radially
4	US 5728131 A	U 19980317	11	Coupling
5	US 5782904 A	U 19980721	9	Intralum
6	US 5824046 A	U 19981020	14	Covered
7	US 5824042 A	U 19981020	23	Endolumi
8	US 5824037 A	U 19981020	28	Modular
9	US 5824034 A	U 19981020	9	Method f
10	US 5843158 A	U 19981201	21	Limited
11	US 6036725 A	U 20000314	14	Expandab
12	US 6110198 A	U 20000829	27	Method f
13	US 6139573 A	U 20001031	19	Conforma
14	US 6193745 B1	U 20010227	28	Modular
15	US 6203568 B1	U 20010320	23	Endolumi
16	US 20010000188	U 20010405	21	Limited
17	US 6224625 B1	U 20010501	6	Low prof
18	US 6245099 B1	U 20010612	16	Selectiv
19	US 20010010012	U 20010726	17	Selectiv
20	US 6270523 B1	U 20010807	13	Expandab
21	US 20010044647	U 20011122	13	Modular
22	US 6334868 B1	U 20020101	6	Stent co
23	US 6336937 B1	U 20020108	27	Multi-st
24	US 20020004677	U 20020110	6	Low prof
25	US 6344054 B1	U 20020205	7	Endolumi
26	US 20020045931	U 20020418	10	Support
27	US 6416522 B1	U 20020709	17	Intralum
28	US 6464719 B2	U 20021015	6	Low prof
29	US 6475232 B1	U 20021105	12	Stent wi
30	US 20020173837	U 20021121	19	Prosthet
31	US 20030065379	U 20030403	13	Reductio
32	US 6547814 B2	U 20030415	16	Selectiv
33	US 6554855 B1	U 20030429	22	Low prof
34	US 20030093145	U 20030515	20	Endolumi
35	US 6565596 B1	U 20030520	11	Intralum
36	US 20030125796	U 20030703	21	Low prof
37	US 6592614 B2	U 20030715	20	Cuffed e
38	US 20030149472	U 20030807	13	Modular

US-PAT-NO: 5443499

DOCUMENT-IDENTIFIER: US 5443499 A

TITLE: Radially expandable tubular prosthesis

----- KWIC -----

## Brief Summary Text - BSTX (10):

In one preferred embodiment, the prosthesis is made from a woven fabric having substantially drawn longitudinal yarns (warp yarns) which ~~are~~ are ~~expansion~~ or elongation of the prosthesis in the longitudinal direction, and radial yarns (fill yarns) which are at most partially drawn to allow for expansion of the prosthesis in the radial direction when the yield point of the radial yarns is exceeded.

## Current US Cross Reference Classification - CCXR (1):

6237.113

US-PAT-NO: 5443499

DOCUMENT-IDENTIFIER: US 5443499 A

TITLE: Radially expandable tubular  
prosthesis

----- KWIC -----

Brief Summary Text - BSTX (10):

In one preferred embodiment, the prosthesis is made from a woven fabric having substantially drawn longitudinal yarns (warp yarns) which limit expansion or elongation of the prosthesis in the longitudinal direction, and radial yarns (fill yarns) which are at most partially drawn to allow for expansion of the prosthesis in the radial direction when the yield point of the radial yarns is exceeded.

Current US Cross Reference Classification - CCXR (1):  
623/1.13

	Document ID	RSC	Issue-Date	Page	T
1	US 5123917 A	U	19920623	9	Expan
2	US 5443499 A	U	19950822	11	Radia
3	US 5653746 A	U	19970805	11	Radia
4	US 5728131 A	U	19980317	11	Coupl
5	US 5782904 A	U	19980721	9	Intra
6	US 5824046 A	U	19981020	14	Cover
7	US 5824042 A	U	19981020	23	Endol
8	US 5824037 A	U	19981020	28	Modul
9	US 5824034 A	U	19981020	9	Metho
10	US 5843158 A	U	19981201	21	Limit
11	US 6036725 A	U	20000314	14	Expan
12	US 6110198 A	U	20000829	27	Metho
13	US 6139573 A	U	20001031	19	Confo
14	US 6193745 B1	U	20010227	28	Modul
15	US 6203568 B1	U	20010320	23	Endol
16	US 20010000188	U	20010405	21	Limit
17	US 6224625 B1	U	20010501	6	Low p
18	US 6245099 B1	U	20010612	16	Selec
19	US 20010010012	U	20010726	17	Selec
20	US 6270523 B1	U	20010807	13	Expan
21	US 20010044647	U	20011122	13	Modul
22	US 6334868 B1	U	20020101	6	Stent
23	US 6336937 B1	U	20020108	27	Multi
24	US 200200004677	U	20020110	6	Low p
25	US 6344054 B1	U	20020205	7	Endol
26	US 20020045931	U	20020418	10	Suppo
27	US 6416522 B1	U	20020709	17	Intra
28	US 6464719 B2	U	20021015	6	Low p
29	US 6475232 B1	U	20021105	12	Stent
30	US 20020173837	U	20021121	19	Prost
31	US 20030065379	U	20030403	13	Reduc
32	US 6547814 B2	U	20030415	16	Selec
33	US 6554855 B1	U	20030429	22	Low p
34	US 20030093145	U	20030515	20	Endol
35	US 6565596 B1	U	20030520	11	Intra
36	US 20030125796	U	20030703	21	Low p
37	US 6592614 B2	U	20030715	20	Cuffe
38	US 20030149472	U	20030807	13	Modul

US-PAT-NO: 5824037

DOCUMENT-IDENTIFIER: US 5824037 A

TITLE: Modular intraluminal prostheses construction and methods

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## Brief Summary Text - BSTX (23):

In yet another aspect, the present invention provides a liner-limited stent-graft comprising a resilient radially expandable tubular frame, and a tubular liner disposed over at least a portion of an inner or outer surface of the frame. The liner ~~limits the resilient expansion~~ of at least a portion of the frame when the stent-graft is in a relaxed state. Advantageously, when the liner is disposed within the frame the tension from the frame provides a smooth prosthetic lumen defined at least in part by a taut liner surface. Furthermore, axial variations in the perimeter of the liner produce axial variations in the stent-graft lumen, even where the frame structure remains axially uniform in diameter. Such liner-limited stent-grafts are particularly well-suited for use with the selective shrinking or plastic expansion of a liner to produce axially tailored endoluminal prosthesis, as described hereinbelow.

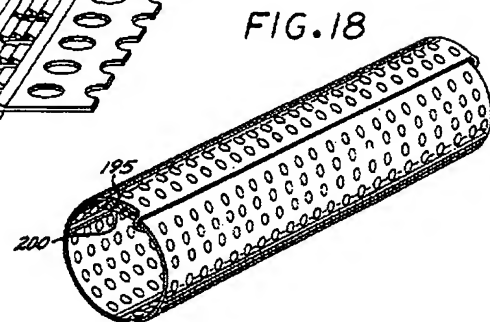
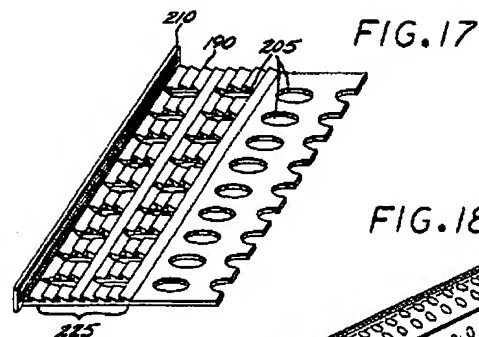
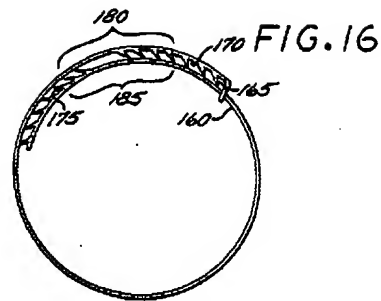
## Detailed Description Text - DETX (27):

A third axially varying prosthesis 130 includes an inelastic inner flared graft 132 which restrains the total diameter of the prosthesis from within the stent through the stent/graft attachment threads. The graft includes a greater perimeter at both ends, allowing the stent rings located in the end portions to expand to a larger diameter. The shape of this prosthesis is particularly well suited for treatment of aneurysms and other weakened vessels, as the flared ends provide secure proximal and distal anchors beyond the aneurysm, while the liner ~~limits expansion~~ of a central portion of the prosthesis to avoid distressing the weakened vessel wall at the aneurysm itself.

## Detailed Description Text - DETX (28):

Graft material is typically highly flexible so that the prosthesis is radially compressible to a narrow diameter configuration for insertion and positioning within a body lumen. However, the graft material is also generally inelastic to avoid any stretching of the liner material after deployment, as excess loose fabric may interfere with the flow through the prosthesis lumen. As seen in each of FIGS. 6A-C, the inelastic liner of the present invention preferably ~~limits the maximum expansion~~ of at least a portion of the resilient frame. Specifically, at least one resilient stent ring 112 in each of axially varying prostheses 110, 120, and 130, does not reach a fully-expanded, relaxed state. Instead, the liner restrains the total exoanded diameter of the

	Document ID	Class	Issue Date	Page	Title
907	US 5800456 A	U	19980901	8	Spiral stent
908	US 5788626 A	U	19980804	12	Method of
909	US 5782906 A	U	19980721	8	Combination
910	US 5779732 A	U	19980714	8	Method and
911	US 5779729 A	U	19980714	4	Coated stent
912	US 5776183 A	U	19980707	7	Expandable
913	US 5776182 A	U	19980707	20	Blood control
914	US 5776181 A	U	19980707	21	Expandable
915	US 5766710 A	U	19980616	12	Biodegradable
916	US 5755782 A	U	19980526	16	Stents for
917	US 5755776 A	U	19980526	11	Permanent
918	US 5755771 A	U	19980526	10	Expandable
919	US 5741293 A	U	19980421	18	Locking stent
920	US 5735897 A	U	19980407	8	Intravascular
921	US 5733330 A	U	19980331	8	Balloon-expandable
922	US 5733303 A	U	19980331	14	Flexible expandable
923	US 5728150 A	U	19980317	15	Expandable
924	US 5725549 A	U	19980310	18	Coiled stent
925	US 5725548 A	U	19980310	5	Self-locking
926	US 5718713 A	U	19980217	10	Surgical stent
927	US 5716981 A	U	19980210	121	Anti-angiogenic
928	US 5700286 A	U	19971223	14	Polymer film
929	US 5697971 A	U	19971216	8	Multi-cell
930	US 5690670 A	U	19971125	17	Stents of
931	US 5674278 A	U	19971007	8	Endovascular
932	US 5672169 A	U	19970930	7	Stent mount
933	US 5653727 A	U	19970805	14	Intravascular
934	US 5649977 A	U	19970722	7	Metal reinforcement
935	US 5649952 A	U	19970722	10	Expandable
936	US 5643312 A	U	19970701	9	Stent having
937	US 5643309 A	U	19970701	13	Cardiovascular
938	US 5632840 A	U	19970527	7	Method of
939	US 5632771 A	U	19970527	17	Flexible stent
940	US 5632763 A	U	19970527	7	Bifurcated
941	US 5630840 A	U	19970520	12	Clad composite
942	US 5630829 A	U	19970520	14	High hoop stress
943	US 5629077 A	U	19970513	9	Biodegradable
944	US 5628787 A	U	19970513	10	Clad composite
945	US 5628785 A	U	19970513	14	Bioelastomer
946	US 5624411 A	U	19970429	13	Intravascular
947	US 5607468 A	U	19970304	7	Method of
948	US 5599352 A	U	19970204	15	Method of
949	US 5591227 A	U	19970107	14	Drug eluting
950	US 5591224 A	U	19970107	14	Bioelastomer
951	US 5591223 A	U	19970107	5	Re-expandable
952	US 5591222 A	U	19970107	9	Method of
953	US 5578075 A	U	19961126	11	Minimally
954	US 5575818 A	U	19961119	13	Endovascular
955	US 5575816 A	U	19961119	9	High strength
956	US 5571166 A	U	19961105	14	Method of
957	US 5551954 A	U	19960903	11	Biodegradable
958	US 5514176 A	U	19960507	8	Pull apart
959	US 5514154 A	U	19960507	11	Expandable
960	US 5449382 A	U	19950912	9	Minimally
961	US 5441515 A	U	19950815	20	Batcheting
962	US 5411551 A	U	19950502	7	Stent assembly
963	US 5411540 A	U	19950502	7	Selective



EAST Browser - L2: (43) (measure of: [US 560923 A] Tag: S   Doc: 5/43 (SORTED)   Format: KWIC					
File	Edit	View	Tools	Window	Help
	Document ID	KS	Issue	Da	Pag
1	US 5394455 A	U	19950228	16	Digit
2	US 5713917 A	U	19980203	26	Appara
3	US 5752522 A	U	19980519	15	Lesion
4	US 5824040 A	U	19981020	35	Endolu
5	US 5860923 A	U	19990118	20	Lesion
6	US 5891192 A	U	19990406	5	Ion-in
7	US 5902308 A	U	19990511	15	Lesion
8	US 5902308 A	D	19990511		Body I
9	US 5948017 A	U	19990907	20	Modula
10	US 5957929 A	U	19990928	12	Expans
11	US 5970119 A	U	19991019	16	Radiol
12	US 5970119 A	D	19991019		Radiol
13	US 5972023 A	U	19991026	23	Implar
14	US 6010511 A	U	20000104	15	Lesion
15	US 6078832 A	U	20000620	20	Lesion
16	US 6084941 A	U	20000704	8	Device
17	US 6099548 A	U	20000808	27	Appara
18	US 6106549 A	U	20000822	21	Modula
19	US 6187015 B1	U	20010213	12	Expans
20	US 20010005793	U	20010628	12	Expans
21	US 6273895 B1	U	20010814	16	Methoc
22	US 6283991 B1	U	20010904	34	Endolu
23	US 6287335 B1	U	20010911	102	Intrav
24	US 6287315 B1	U	20010911	27	Appara
25	US 20010027338	U	20011004	11	Endova
26	US 20010047198	U	20011129	104	Intrav
27	US 6334869 B1	U	20020101	25	Endolu
28	US 20020026210	U	20020228	18	Endova
29	US 20020065545	U	20020530	28	Appara
30	US 20020068967	U	20020606	104	Intrav
31	US 6406487 B2	U	20020618	12	Expans
32	US 20020077634	U	20020620	28	Methoc
33	US 20020120327	U	20020829	36	Endolu
34	US 6451051 B2	U	20020917	100	Intrav
35	US 20020151954	U	20021017	13	Expans
36	US 20020165572	U	20021107	22	Emboli
37	US 20020183629	U	20021205	11	Implar
38	US 20020183628	U	20021205	13	Pressu
39	US 20030004562	U	20030102	13	Endolu
40	US 20030125790	U	20030703	12	Deploy
41	US 6592612 B1	U	20030715	26	Methoc
42	US 20030136417	U	20030724	25	Implar
43	US 20030149368	U	20030807	11	Methoc

the length of the aneurysm can be determined by reading the calibration marks 30.

#### Detailed Description Text - DETX (18):

Referring to FIGS. 7-11, an exemplary method for measuring the length of a vascular aneurysm in a blood vessel 54 will be described. The method will be described with reference to the catheter 10 employing the centering balloon 44 as shown in FIG. 5. As shown in FIG. 7, the guidewire 40 is initially introduced into the vessel 54 so that it passes through the aneurysm 56. The catheter 10 is then advanced along the guidewire 40 while held within the third member 50 until a proximal end 58 of the aneurysm 56 is reached. Conventional fluoroscopy procedures are employed to visualize the radiopaque markers 18, 26 and the aneurysm 56. The catheter 10 is adjusted until the radiopaque marker 18 is aligned with a target location at the proximal end 58 of the aneurysm 56. Preferably, the target location will be at about 0.5 cm to 10 cm from the aneurysm 56. Such a distance provides sufficient space for placement of a proximal end of a graft. As shown in FIG. 8, the third elongate member 50 can optionally be radially expanded or have a malecot actuated to center the catheter 10 within the vessel 54.

#### Detailed Description Text - DETX (24):

A further advantage of the catheter 70 is that both the diameter and the orientation of the markers 78 in the lumen can be determined. For example, an ultrasonic imaging transducer can be inserted through lumen 74 where it can be rotated to determine the diameter of the markers 78 and the distance between each of the markers 78. Ultrasound can be used with either an elastic or an inelastic balloon 76. Use of ultrasound is advantageous in providing excellent data acquisition. The resulting dimensions can then be used to construct a dimensionally significant graphical representation, such as a three dimensional wireframe model, of the markers 78. Such a model would yield the length, diameter, and radius or curvature of the body lumen and could be used in the selection of an appropriately sized prosthetic device, such as a stent graft for treating aneurysmal disease.

	Document ID	RS	Issue-Date	Page	Title
1	US 5394455 A	U	19950228	16	Digit
2	US 5713917 A	U	19980203	26	Appara
3	US 5752522 A	U	19980519	15	Lesion
4	US 5824040 A	U	19981020	35	Endolu
5	US 5860923 A	U	19990119	20	Lesion
6	US 5891192 A	U	19990406	5	Ion-in
7	US 5902308 A	U	19990511	15	Lesion
8	US 5902308 A	D	19990511		Body I
9	US 5948017 A	U	19990907	20	Module
10	US 5957929 A	U	19990928	12	Expans
11	US 5970119 A	U	19991019	16	Radiol
12	US 5970119 A	D	19991019		Radiol
13	US 5972023 A	U	19991026	23	Implar
14	US 6010511 A	U	20000104	15	Lesion
15	US 6078832 A	U	20000620	20	Lesion
16	US 6084941 A	U	20000704	8	Device
17	US 6099548 A	U	20000808	27	Appara
18	US 6106549 A	U	20000822	21	Module
19	US 6187015 B1	U	20010213	12	Expans
20	US 20010005793	U	20010628	12	Expans
21	US 6273895 B1	U	20010814	16	Method
22	US 6283991 B1	U	20010904	34	Endolu
23	US 6287335 B1	U	20010911	102	Intrav
24	US 6287315 B1	U	20010911	27	Appara
25	US 20010027338	U	20011004	11	Endova
26	US 20010047198	U	20011129	104	Intrav
27	US 6334869 B1	U	20020101	25	Endolu
28	US 20020026210	U	20020228	18	Endova
29	US 20020065545	U	20020530	28	Appara
30	US 20020068967	U	20020606	104	Intrav
31	US 6406487 B2	U	20020618	12	Expans
32	US 20020077634	U	20020620	28	Method
33	US 20020120327	U	20020829	36	Endolu
34	US 6451051 B2	U	20020917	100	Intrav
35	US 20020151954	U	20021017	13	Expans
36	US 20020165572	U	20021107	22	Emboli
37	US 20020183629	U	20021205	11	Implar
38	US 20020183628	U	20021205	13	Pressu
39	US 20030004562	U	20030102	13	Endolu
40	US 20030125790	U	20030703	12	Deploy
41	US 6592612 B1	U	20030715	26	Method
42	US 20030136417	U	20030724	25	Implar
43	US 20030149368	U	20030807	11	Method

Methods and apparatus are therefore needed for accurately measuring the cross-section of a body lumen, and in particular the diameter, circumference, and cross-sectional area of a vascular lesion. In one particular aspect, it would be desirable to provide improved methods and apparatus for the measurement of blood vessels in the region adjacent aneurysms so that the proper size of intraluminal prostheses, such as grafts and stents, can be accurately determined. It would be further desirable if such methods and apparatus were simple to use and could be used with existing fluoroscopy technology. Finally, it would be particularly desirable if such measurements could be taken without causing unnecessary stress to the diseased vessel.

Brief Summary Text - BSTX (16):

The present invention provides methods and apparatus for determining a cross-sectional dimensions of body lumens, and particularly for determining the cross-sectional area, circumference and diameter of target regions within body lumens. Body lumens amenable to the methods and apparatus of the present invention include blood vessels, the intestines, the urethra, and the like. Although suitable for the measurement of most body lumens, the present invention will find its greatest use in the measurement of vascular lesions, particularly vascular aneurysms, vascular stenoses, and the like. Advantageously, the cross-sectional dimensions of such lesions can be used to select the proper size of intraluminal prostheses, such as grafts and stents, the proper balloon for balloon angioplasty procedures, and the proper therapy for that vascular lesion.

Detailed Description Text - DETX (2):

The present invention provides methods and apparatus for determining cross-sectional dimensions, such as the internal diameter, circumference, or cross-sectional area, of a body lumen. The methods and apparatus will preferably be used to measure the cross-section of vascular lesions, and will find its greatest use in measuring the diameter of vascular aneurysms and stenoses. The methods and apparatus can also find use in measuring internal dimensions of other defects or abnormalities. Diameter and peripheral lengths provided by the present invention will be particularly useful in sizing intraluminal prostheses, such as vascular grafts or stents, that are endovascularly placed within the vessel to treat the aneurysm or other abnormality. Cross-sectional areas provided by the invention can also be used to select the proper diameter for a balloon angioplasty catheter or to size other therapeutic devices.

Detailed Description Text - DETX (11):

As shown in FIG. 2, catheter 10 has been inserted within an abnormal lumen 30 and aligned with a target region 32. The diameter of target region 32 might, for example, be needed to determine the size of an intraluminal stent to be inserted within lumen 30. Balloon 20 is shown inflated, thereby blocking a normal blood flow F. Thus the pressure and flow acting on external sensor 24 has been altered. This information is transmitted to the physician via wire



A method of fabricating a helical stent-graft 71 will be described with reference to FIG. 5E. A series of linked diamond-shaped elements 73 are first attached to a strip of liner material 75, typically being stitched with a sewing machine. The ribbon is then wound over a mandrel 77 of the desired size, and adjacent edges of the ribbon are sewn to each other (or otherwise permanently joined). Such a method may be substantially automated and continuous, and is thus particularly beneficial for producing a large number of prostheses. The helical stent-graft may optionally be cut to length, but will preferably include a crown stitched stent-ring 79 for sealing and ends against a surrounding lumen when deployed therein.